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Conflicts of interest

B.N.L. and R. V. are shareholders in Nemo Healthcare BV, the Netherlands. R.K. is employed by Nemo Healthcare BV; M.G. F. is an inventor of related patent application entitled “EEG Monitor of Fetal Health” including U.S. Patent 9,215,999. M.G.F. co-filed a patent for the aECG method referred to in this article; The remaining authors report no conflict of interest.
Abstract

The second Signal Processing and Monitoring in Labor workshop gathered researchers who utilize promising new research strategies and initiatives to tackle the challenges of intrapartum fetal monitoring. The workshop included a series of lectures and discussions focusing on: new algorithms and techniques for cardiotocography (CTG) and ECG acquisition and analyses; the results of a CTG evaluation challenge comparing state-of-the-art computerized methods and visual interpretation for the detection of arterial cord pH<7.05 at birth; the lack of consensus about the role of intrapartum acidemia in the etiology of fetal brain injury; the differences between methods for CTG analysis ‘mimicking’ expert clinicians and those derived from ‘data-driven’ analyses; a critical review of the results from two randomized controlled trials testing the former in clinical practice; and relevant insights from modern physiology-based studies.

We concluded that the automated algorithms performed comparably to each other and to clinical assessment of the CTG. However, the sensitivity and specificity urgently need to be improved (both computerized and visual assessment). Data-driven CTG evaluation requires further work with large multicenter datasets based on well-defined labor outcomes. And before first tests in the clinic, there are important lessons to be learnt from clinical trials that tested automated algorithms mimicking expert CTG interpretation. In addition, transabdominal fetal ECG monitoring provides reliable CTG traces and variability estimates; and fetal ECG waveform analysis is subject to promising new research.

There is a clear need for close collaboration between computing and clinical experts. We believe that progress will be possible with multidisciplinary collaborative research.

Keywords

Health data; sensitivity; specificity; artificial intelligence; Cardiotocography; electronic fetal monitoring; intrapartum care; hypoxic-ischemic encephalopathy.
**Abbreviations**

FHR – fetal heart rate;

CTG – cardiotocography;

ECG – electrocardiogram;

HIE – hypoxic ischemic encephalopathy;

SPaM in Labour – Signal Processing and Monitoring in Labour;
Introduction

Continuous fetal heart rate (FHR) monitoring with cardiotocography (CTG) remains the mainstay of intrapartum fetal surveillance. Its intended goal is to prevent death or hypoxic-ischemic encephalopathy (HIE), by identifying incipient hypoxia/ischemia in a previously healthy fetus, at a time when intervention can prevent or mitigate permanent injury. Its goal is not considered to be the identification of infection during labor or trauma related to the delivery. While pre-existing injury, anomaly or antenatal hypoxia may be suspected, on the basis of a deviant FHR pattern, it is unknown whether the injury associated with these factors can be mitigated or aggravated by obstetrical care during labor. Nonetheless, these factors modulate the risk of neural injury and can influence the FHR trace, along with the timing and urgency of delivery. In addition, HIE does not represent either a single clinical picture or pathogenesis. Injury evolves over hours and its physiological manifestations (in FHR changes or other signs) are not confined to a single short period of time\(^1\). On the other hand, some injurious events develop precipitously and show non-standard FHR and/or neuroradiological patterns\(^2\). These occurrences may not be preventable but emergency operative delivery may still be warranted. For example, in order to start hypothermia treatment promptly; or in order to prevent exacerbating the injury by allowing the labor to continue.

Evidence has been available for nearly half a century that FHR abnormalities are often not related to fetal acidosis\(^3,4\). As a result, the rate of unnecessary operative deliveries is high\(^5,6\) with adverse implications for this and/or subsequent pregnancies. Furthermore, even experts disagree with each other when interpreting the intrapartum FHR (for example, Chauhan et al\(^7\)). Clinical guidelines that focus on the CTG morphology in isolation, encourage clinicians to conclude that every FHR pattern has a single and straightforward correct interpretation\(^8\). In reality, often complex interactions between multiple clinical factors need to be taken into account.

Recent randomized clinical trials for novel intrapartum monitoring technologies have largely failed to show improvement in neonatal outcomes when compared to current visual-based CTG monitoring\(^9-11\). But large clinical retrospective studies of intrapartum computer-aided FHR interpretation (mimicking clinical experts) in conjunction with other technologies, are more optimistic\(^12,13\) (38,466 and 78,456 births in the respective studies). With no other surveillance modalities on the horizon and the raise of artificial intelligence and data analytics for healthcare, now is the time to create opportunities for multidisciplinary joint efforts, pushing
new boundaries in an attempt to move forward. For example, FHR algorithms that harness the complex information from large clinical datasets are under development and have never been tested in the clinic: Georgieva et al 2017, using data from 22,000 births demonstrated that a very simple data-driven system compares favorably to clinical CTG evaluation in prediction of several types of poor neonatal outcome. With larger datasets and more sophisticated methods, we expect that such systems would evolve to play an invaluable role in the future of intrapartum FHR analysis. Further research is needed to test this hypothesis.

These algorithms cannot be developed in a vacuum. Indeed a number of related factors require consideration. Obstetrical decisions relate to two independent organisms where efforts to benefit one may be harmful to the other; the preventability of injury; the feasibility of safe vaginal delivery; the trajectory of deterioration; the need to defend against allegations of malpractice; the need for urgent delivery and the maintenance of a reasonable frequency of cesarean delivery, and more. But there is a clear need for reliable and objective technologies to monitor and help clinicians identify the fetus at risk during labor.

This gives the motivation for the bi-annual Workshop on Signal Processing and Monitoring (SPaM) in Labor, where a broad range of multidisciplinary new research strategies and initiatives are considered. The aims of the SPaM Workshop are to provide "a truly multidisciplinary forum and spirit and common language for clinicians, physiologists and signal processing researchers". Registration through the website of the workshop is open to everybody willing to attend. Opportunity is given to anyone willing to give a talk on a relevant subject with ample time for discussions and questions. There have been no abstract submissions or proceedings so far. We gathered participants from Europe, USA, Canada, and New Zealand, including experts from obstetrics, engineering, computer science; machine learning; physiology, physics and epidemiology. There were representatives from the producers of fetal monitors (Phillips, GE/Monica Healthcare, Huntleigh Healthcare, Nemo Healthcare and Laerdal Medical) and medical or engineering students.

This paper is designed to provide a current review of computer-based methods for continuous fetal monitoring and relevant clinical trials; set a benchmark of state-of-the-art performance of such methods on multicentre data; critically examine the most important obstacles and

Workshop webpage: https://www.wrh.ox.ac.uk/research/spam-in-labour
controversies impeding progress; sign-post the reader to the newest relevant research; and outline the most promising future directions for research.

**Structure and main topics of the workshop**

In this paper, we review the main themes and ideas of the meeting, rather than individual presentations, which are available through the workshop webpage. The workshop discussions gravitated around the following main topics:

1. The concepts of computerized fetal heart rate monitoring: ‘mimicking’ clinicians versus ‘data-driven’ interpretation;
2. The SPaM’17 CTG challenge: evaluation of computerized methods with respect to cord acidemia at birth and visual clinical interpretation;
3. Defining the endpoint(s) of intrapartum monitoring: the ‘good’ and ‘bad’ labor outcomes;
4. Signal processing methods for data-driven computerized CTG;
5. Visual-aid computerized CTG: lessons from randomized clinical trials;
6. Trans-abdominal fetal electrocardiogram monitoring;
7. Fetal physiology in the age of big data;
8. Beyond fetal heart rate: emerging technologies and adoption challenges;
9. Bringing new monitoring modalities to the market.

**Themes highlighted during the workshop**

1. The concepts of computerized fetal heart rate monitoring: ‘mimicking’ clinicians versus ‘data-driven’ interpretation

Two approaches to computerized CTG analysis have been developed in the past: (a) systematic visual assessment to identify classic CTG features such as baseline, variability, decelerations/accelerations, contractions, with alerts based on clinical guidelines; (b) data-driven methods that use routinely collected CTG and fetal health data to investigate signal processing-based metrics and/or interpretation methods that best relate to measures of fetal wellbeing and labor outcome. The data-driven concept is based on analyzing a very large number of records (at the very least a few thousands, but as the next decade of ‘big data’ unfolds, even millions of CTGs); with the capacity of learning to recognize rare events, such as hypoxic-ischemic encephalopathy. Below in theme 4, these emerging methods are reviewed in more detail and the reader is signposted to the relevant literature.
The visual-aid methods, which have been evaluated in two randomized clinical trials discussed below, have the potential to reduce the lack of objectivity, limited availability or training of clinical staff, and human error/fatigue. In contrast, with larger FHR/CTG datasets and increasing computing power, researchers can now focus on data-driven methods (reviewed below). Data-driven approaches tackle the same issues as the visual-aid approaches but also directly aim to improve the detection of infants at high risk for intrapartum compromise, learning from vast amounts of data. Such methods are still undergoing development and none have been tested in clinical studies yet. Therefore, we underline the fundamental difference between the two computer-based approaches to FHR evaluation.

2. The SPaM’17 CTG challenge: evaluation of computerized methods with respect to cord acidemia at birth and visual clinical interpretation

A multicenter dataset was assembled before the workshop, and is now available at the Workshop webpage. This SPaM’17 database comprises 300 labors collected from three participating centers (Lyon, France; Brno, Czech Republic; and Oxford, UK). Each center provided 100 cases: 80 with arterial cord pH in with values within 7.25-7.30 and 20 with arterial cord pH<7.05. Only cases with validated cord gases were included (arterial pH < venous pH – 0.02). The goal was to “evaluate state-of-the-art algorithms for prediction of low umbilical artery pH at birth from intrapartum CTG recordings”. Included were only singleton pregnancies of more than 36 weeks gestation. Excluded were small for gestational age babies and those with congenital abnormalities. Selected were only CTGs longer than 60 minutes, with less than 15% signal loss and ending within ten minutes of birth. All CTGs were acquired as part of standard clinical practice at the respective units, with standard CTG monitors and the FHR was only available to the researchers uniformly sampled at 4Hz, as per standard manufacturing. Teams were allowed up to five submissions and were informed about their ‘score’, calculated as the square root of Sensitivity (Se) multiplied by Specificity (Sp). Se and Sp were also reported and discussed at the workshop.

Overall, eight teams participated and had comparable performance. Two teams used the SPaM’17 dataset as a ‘training’ dataset, informing their algorithms development according to the obtained score and two teams used the dataset to test new applications of algorithms, still under development (no relevant publications). The remaining four teams used established algorithms for CTG analysis that had been developed and tested prior to the challenge: SisPorto
4.0 incorporating the FIGO clinical guidelines\textsuperscript{14}; Phase Rectified Signal Averaging (OxSys 1.0), tuned using over 7,000 CTGs from Oxford\textsuperscript{5,15}; Sparse Support Vector Machines trained using over 1800 CTGs from Lyon\textsuperscript{16,17}; Auto mutual information applied only to the last 30min of first stage labor, and was tuned using over 900 CTGs from Lyon\textsuperscript{18}. Summary statistics of the Se and Sp values for the latter four methods are shown in Table 1. There was a substantial variance of performance of all algorithms with respect to where the data came from (Oxford, Brno or Lyon), underlying the importance of multicenter datasets.

Table 1. SPaM’17 CTG challenge: performance in detecting arterial cord pH<7.05 of the four established methods: SisPorto 4.0\textsuperscript{14}; OxSys 1.0\textsuperscript{5,15}; Sparse Support Vector Machines\textsuperscript{16,17}; Auto mutual information\textsuperscript{18}. Oxford, Lyon and Brno provided 100 CTGs each: 20 with arterial cord pH<7.05 and 80 with pH>7.25. The number of true positives and true negatives can then be calculated by dividing the numbers in the Table by five.

<table>
<thead>
<tr>
<th>Median (Min-Max)</th>
<th>Sensitivity (%)</th>
<th>Specificity (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Oxford data subset</td>
<td>62.5 (55-65)</td>
<td>74 (64-84)</td>
</tr>
<tr>
<td>Lyon data subset</td>
<td>77.5 (75-95)</td>
<td>76 (60-78)</td>
</tr>
<tr>
<td>Brno data subset</td>
<td>55 (45-65)</td>
<td>71.5 (70-72)</td>
</tr>
<tr>
<td>All data</td>
<td>65 (60-73)</td>
<td>73 (70-74)</td>
</tr>
</tbody>
</table>

Twenty selected CTGs from the 300 were also evaluated by five clinicians, blinded to outcome. These were the ones for which the automated methods had the highest disagreement between themselves and/or majority did not predict correctly the labor outcome. Ten of the 20 had arterial cord pH < 7.05. The obstetricians were asked to identify the cases which are likely to have arterial cord pH < 7.05 and/or require early operative delivery. No other information, but the CTG was provided. The images of CTGs were provided in both EU standard (1cm/min) and US standard (3cm/min), one US-based and four EU-based doctors responded to the challenge. Four of the clinicians are currently practicing obstetricians consultants in Europe (UK, Portugal and the Czech Republic) and one is US-based. They all have both clinical and academic interest in CTG interpretation.

The main results from the visual evaluation for the prediction of arterial cord pH < 7.05 could be summarized as follows:
- All five clinicians agreed with each other in five out of the 20 CTGs; only four clinicians agreed with each other for nine out of 20; and only three clinicians were in agreement for the remaining six CTGs.

- Majority vote (MV) of the automated methods agreed with MV of the clinicians in 85% (17 out of 20) of the selected CTGs. For the remaining three cases, the clinical MV correctly predicted the outcome whereas the automated methods’ MV did not.

- MV(algorithms) and MV(clinicians) agreed but did not correctly predict the labor outcome in six cases: four were false negatives and two were false positives.

The controversial nature of CTG evaluation was evident not only in the results of the challenge but during their discussion at the workshop’s dedicated session. Firstly, defining labor outcome by cord gas analyses was deemed unsuitable by some of the participants (as discussed in detail below in Section 3). Secondly, the clinicians were visibly challenged to discuss their CTG interpretation in this kind of competitive manner, especially with no clinical context provided (but this was required in order to compare fairly to automated methods). Moreover, many of the active clinical participants in the workshop did not submit formally their evaluations.

We concluded that, generally speaking, the automated algorithms perform comparably to each other and to clinical assessment of the CTG (with no clinical context). It is important that data from multiple hospitals is used. Most importantly, Se and Sp urgently need to be increased by future work (both computerized and visual assessment). But we note that, the optimal Se and Sp that (in theory or practice) could be achieved by the best possible CTG interpretation, remain unknown and heavily depend on the way fetal compromise is defined (discussion in the next section).

3. Defining the endpoint(s) of intrapartum monitoring: the ‘good’ and ‘bad’ labor outcomes

Without defining and quantifying the outcomes of labor that we want to prevent, we cannot assess whether one method for monitoring is better than another, and ultimately cannot progress. The issue of how to define the relevant outcomes has been one of the most important and debated problems during the SPaM workshops. There remains no clarity or consensus about the goal of intrapartum CTG monitoring, in particular, the role of intrapartum acidemia in the etiology of fetal brain injury which remains one of the biggest challenges in data-driven
About two thirds of speakers at the workshop used a single cord gas parameter in their research (pH or base deficit). Fetal acidosis at birth is a risk factor for clinically important neurological outcomes such as convulsions and neonatal encephalopathy, but a large proportion of newborns with very low pH / high base deficit values are clinically well and do not require special neonatal care. The remaining third of researchers used hypoxic-ischemic encephalopathy (HIE) or composite outcomes as endpoints of intrapartum CTG. The adopted definition of HIE was confounded by including acidemia as a requirement for HIE (discussions of the ways to define HIE can be found in Kurinczuk et al., ACOG 2014, Leviton et al and the references therein). Importantly, the acidemia prerequisite for HIE diagnosis, leaves out of the analysis the newborn with brain injury, but normal cord gases at birth. Highlighted was the importance of complex intrapartum factors such as maternal fever, infection, meconium, growth restriction, pre-existing injury. These and/or other risk factors may perturb fetal cerebral function and FHR patterns in the absence of acidemia. Further understanding of these and other factors, their effect on intrapartum FHR and how they modulate the utility of current/future biomarkers of hypoxic-ischemic injury is urgently needed. If the importance of cord blood gas analysis is to be reduced, what indices of labor outcome can be objectively measured to assess the impact of improved CTG analysis? And, from the point of view of data-driven methods, there may well be the need for different algorithms to detect these heterogeneous pathophysiological mechanisms, which may manifest themselves differently in the FHR pattern.

These complexities underline the clear need for close collaboration between computing and clinical experts, and the need for research/time before tangible results could be achieved.

4. Signal processing methods for data-driven computerized CTG

Figure 1 provides a general overview for the concepts in applying computers for signal processing and machine learning for data-driven computerized CTG. We note that the principles illustrated here are by no means unique to CTG, but they underline most situations where we teach the computers to recognize and analyze complex real-world information, i.e. developing artificial intelligence for decision support. The key concepts are: availability of data to learn from (training and testing datasets); signal feature extraction and selection (finding the
most important information in the data); machine learning to classify the CTG signals (use that information to achieve as good as possible accuracy, i.e. develop mathematically *optimal* methods); and the relatively new and quickly developing field of deep learning where feature extraction, selection and machine learning are (in a way) fully automated and *optimized* by a super-computer.

Figure 1. Overview of the concepts for data-driven CTG analysis.

(1) Feature extraction

Clinical guidelines for CTG analysis are derived from the International Federation of Gynecology and Obstetrics (FIGO) or similar sources. They focus on the three main FHR characteristics, namely, baseline rate (level, trend), decelerations/accelerations (frequency,
shape, depth, duration), and variability (long- or short-term). It is well appreciated that visual assessment of these criteria suffers from significant intra- and inter-observer variability\textsuperscript{24} and leads to unnecessary operative deliveries\textsuperscript{25}.

Besides the automated analysis of temporal patterns inspired by FIGO criteria, FHR temporal dynamics have been further assessed by spectrum estimation; i.e., the repartition of energy as a function of frequency, in the range 0.04 to 2Hz, with the calculation of high frequency (HF) and low frequency (LF) energies or LF/HF ratio, quantifying a putative sympathovagal balance in fetuses\textsuperscript{26}. Further, more advanced statistical signal processing tools have been used, probing either nonstationarities (time-frequency), scale-free dynamics (wavelets, fractal) and/or nonlinear mechanisms and hence dependencies beyond the mere correlation (bispectrum, information theoretic measures, entropy rates, multifractal analysis, scattering transforms, conditional statistics as in the Phase Rectified Signal Analysis method\textsuperscript{15,16,18,27-30}). These result in many different FHR features/characteristics. Yet, it is generally well accepted that, on their own, FHR changes are not enough for use in clinical practice and a recent review re-emphasized the need for the wider clinical picture in the interpretation and management of FHR patterns during labor\textsuperscript{31}. Therefore, Georgieva et al.\textsuperscript{5} presented a basic system prototype to assess the CTG, based mainly on one feature (the Phase Rectified Signal Averaging), but adjusted the analysis to clinical risk factors and achieved performance comparable to that of clinical practice (applied to the CTGs of over 22,000 births). Georgieva et al.\textsuperscript{5} demonstrated that such ‘hybrid’ approaches (that combine CTG metrics with other risk factors) are likely to lead to better performance of the classifiers, but require reliable documented clinical data (e.g. that of maternal comorbidities).

(2) Feature selection and classification (machine learning)

Machine learning for classification into normal or abnormal has included several methods for automated ‘classification’, such as Bayesian\textsuperscript{32}, Support Vector Machines\textsuperscript{33,34}, Random Forest, and Artificial Neural Networks\textsuperscript{35}, and often involved almost all proposed features. However, different features may often provide redundant/correlated information. Whereas, joining feature selection and optimal classification into one step, has demonstrated that a few well-chosen features are as efficient as rules involving many features\textsuperscript{16,17,34}. In addition, it can be shown that FHR interpretation rules for the first and active-pushing stages of labor may need to be different\textsuperscript{16,17}.

(3) Deep Learning approaches
Finally, FHR analysis would benefit from the wider availability of large, documented and shared databases that permit robust evaluation of detection/performance of different machine learning methods. In particular, such data could be used with approaches based on ‘deep learning’ strategies\textsuperscript{36,37}. These are powerful, next generation artificial intelligence approaches, where the computers independently seek what is important in the data and do not rely on human-derived features/characteristics. For example, preliminary work by Petrozziello et al. 2018\textsuperscript{36} demonstrates that convolutional neural networks, trained with the data from 30,000 labors at term, have promising performance; and their accuracy and robustness increase with the size of the training dataset\textsuperscript{36}.

In summary, data-driven FHR interpretation needs further research and will benefit from larger datasets based on well-defined labor outcomes which include clinically relevant risk factors and co-morbidities. With a longer-term view and the introduction of full electronic patient records in the developed countries, we anticipate that CTG databases available for research could grow to hundreds of thousands of cases, and even millions. In the UK alone, over 300,000 labors at term are monitored with CTG each year currently.

5. Visual-aid computerized CTG: lessons from randomized clinical trials

Two systems comparing computerized CTG analysis to visual assessment were recently evaluated in multicenter randomized trials in the United Kingdom. The FM-Alert trial\textsuperscript{21} assessed the Omniview-SisPorto\textsuperscript{®} 3.5 system\textsuperscript{36} in 7,730 pregnant women at term. The system analyses both CTG and ECG signals (ST-analysis) and provides real-time alerts when features are suggestive of fetal hypoxia/acidosis. There was no overall reduction in the rates of metabolic acidosis (16 (0.40%) vs 22 (0.58%), RR 0.69 [0.36-1.31]) nor in obstetric interventions; in higher risk groups of women, with complications preceding or arising de novo during pregnancy, it may confer benefit. There was a lower than expected rate of newborn metabolic acidosis – the primary outcome - in both arms of the trial.

The INFANT Trial\textsuperscript{11} evaluated the INFANT (K2 Medical Systems) – decision-support software\textsuperscript{38,39}. In this unmasked Randomized Clinical Trial (RCT), 47,062 pregnant women were randomly assigned to the computerized CTG group or the standard clinical care group. No differences were found in the incidence of poor neonatal outcome (a composite outcome for intrapartum stillbirth or, early neonatal death, or neonatal encephalopathy, neonatal unit admission within 24h for ≥ 48h with evidence of feeding difficulties, respiratory illness, or
encephalopathy with evidence of compromise at birth) between the groups (172 (0·7%) vs 171 (0·7%), adjusted RR 1.01, 95% CI 0.82–1.25)). At two years of age, no significant differences were noted in developmental scores.

Neither trial found evidence for benefit from using the computerized systems to improve neonatal outcomes. Both encountered the same issue of a lower than expected incidence of the primary adverse outcome. This may have been caused by staff learning from exposure to the decision-support arm of the trial, resulting in improved outcomes in the control arm (Hawthorne effect). Other methodological issues including multiple comparisons, strengths of findings and plausibility, and the evaluation of the significant findings in secondary outcomes were discussed at a dedicated workshop session with the following conclusions:

(1) CTG in labor is a screening tool, not a therapeutic device or drug. It is unlikely to improve outcomes unless it is followed by effective, necessary interventions. This depends on many factors including clinician performance, resources and training. Neither trial defined clinical actions in response to the alerts. It is also not clear if alerts were ignored: in the INFANT Trial, the median time from identification of the last “red” alert to birth, was 13–279 min across different units, suggesting disparate approaches to severe CTG abnormalities. A standardized, specified list of actions (such as delivery or not; discontinuation of oxytocin infusion) in response to well-defined CTG and uterine activity patterns, combined with post-hoc monitoring of compliance, could be considered in future trials.

(2) The Hawthorne Effect. If both INFANT and FM-Alert improved staff FHR interpretation skills, these benefits may be extended to the care of women in the control arms thereby contaminating them. This could be prevented in future trials by using a cluster randomized methodology.

(3) Future RCTs should have a period of pre-randomization benchmarking of outcome data. In these trials there was a missed opportunity to evaluate outcome data from low risk women who did not have continuous monitoring and from high-risk women who had continuous monitoring with standard care only40.

(4) The studies reported a very low incidence of poor perinatal outcomes, including stillbirths, perinatal brain damage or neonatal death, compared to rates found in UK Obstetric Units41. Similar findings have been reported by others42,43 meaning studies may be underpowered to detect the predefined differences. It appears that women participating in studies evaluating intrapartum fetal monitoring have better perinatal outcomes; this suggests that there is an
urgent need to improve knowledge and training regarding appropriate responses to CTG abnormalities in general.

(5) Do the specific algorithms used by the evaluated systems simply not work? Both systems identified fetal heart-rate abnormalities; however, the alerts did not take into account other data from labor such as its progress, maternal fever, chorioamnionitis or the presence of meconium. More importantly, algorithms mimicking clinicians cannot be expected to work better than the best clinical expert. This is unlike data-driven algorithms that have the potential to learn from vast amounts of past data. Unfortunately, there was no provision to store and make data available to research beyond the RCT in INFANT. However, the team behind the FM-Alert trial are putting efforts to obtain and use the data from their trial for further research.

In summary, we should consider the discussed complexities when designing intrapartum fetal monitoring RCTs. Large and well conducted clinical observational studies 12,13 may be a technical and financially attractive alternative to produce good scientific evidence for new technologies in the field.

6. Trans-abdominal fetal electrocardiogram monitoring

The fetal electrocardiogram (ECG) can be measured non-invasively by positioning electrodes on the abdomen of a pregnant woman44-46. The key challenge is to suppress interference from the maternal ECG. Recent studies confirm that this challenge can be successfully addressed by advanced signal processing methods47,48. Assessment of the fetal ECG has the potential to provide accurate information on FHR variability and enable ECG morphology analysis. Especially via computerized analysis5,49-51, fetal ECG may be able to provide risk assessment on fetal compromise better than possible when using FHR variability obtained via Doppler ultrasound52.

In particular, CTG is bound by a lower temporal precision in identifying beat-to-beat information (fetal heartbeat information derived with ultrasound or fetal scalp electrode by standard monitors at a uniform frequency of ~4Hz). True beat-to-beat data is needed for some of the derivative estimates of the FHR variability with a potential to improve the prediction of neonatal outcomes53. Its utility remains to be investigated in the future with the advance of transabdominal technologies and appropriate data collection. In addition, the question remains whether the within monitor internal pre-processing of the data, which may vary from vendor to vendor, has any impact on automated FHR variability estimation. But technological
advancement in isolation may not solve the utility of FHR variability and we need to understand in what situations it is useful, given the complex nature of FHR variability and its relation to fetal compromise (discussed in the next section). Also, any risk assessment could be complemented with further screening for metabolic acidosis\textsuperscript{54,55} or even congenital heart disease\textsuperscript{56}.

To complement analysis of FHR variability, morphological analysis of the fetal ECG could potentially play a crucial role. This remains to be investigated, and we underline the need to collect relevant data that can be used to address this question. Furthermore, because fetal position affects ECG morphology analysis and the positioning of abdominal electrodes is unknown with respect to fetal orientation (i.e. fetal heart axis), multi-lead ECG recordings are necessary to correct for fetal orientation. Multiple leads allow correction for inter-patient variations in, for example, the fetal electrical heart axis, which may be vital for the detection of fetal metabolic acidosis\textsuperscript{44}.

Finally, transabdominal electrophysiological monitoring can also provide information on uterine activity during labor. Conventional CTG interpretation considers variations in FHR in presence/absence of uterine contractions and recent studies have shown that also computerized CTG interpretation benefits from reliable information on uterine activity\textsuperscript{36,37}. The current standard for non-invasive assessment of uterine activity relies on the tocodynamometer, a strain gauge held in place on the abdomen by a belt. This tocodynamometer typically provides low-quality signals\textsuperscript{57} and its performance degrades for higher body-mass-index (BMI) of the laboring women\textsuperscript{58}. With transabdominal monitoring, information on uterine activity can be calculated that has been shown to have good correlation with intra-uterine pressure\textsuperscript{59,60}. Moreover, the quality of the transabdominal uterine signals is not affected by BMI\textsuperscript{61}.

Compared to standard fetal monitoring technologies, transabdominal fetal ECG monitoring is completely noninvasive and entirely avoids the issue of transducer re-positioning\textsuperscript{58}.

To sum up, transabdominal fetal ECG can already estimate FHR variability more accurately than CTG. It is truly non-invasive and does not expose the fetus to ultrasound waves. The capability for morphological analysis of fetal ECG waveform is advancing, but there needs to be more research in the interpretation of these waveforms, with or without associated FHR analysis.

7. Fetal physiology in the era of big data
The original introduction of CTG was tightly linked to the underlying physiology and indeed many of the pioneers of CTG undertook seminal physiological studies, which continue to guide the way clinicians, physiologists and now engineers and computer scientists approach CTG interpretation. One of the founding principles of CTG interpretation was that decelerations have multiple etiologies some of which are benign. Distinguishing these ‘benign’ early decelerations from ‘pathological’ late decelerations and the sometimes-pathological variable decelerations was therefore important. Another key principle was that suppressed FHR variability (FHRV) appeared to be the most consistent predictor of neonatal acidemia.

This original physiology-driven approach is now being refined by data-driven approaches. Intriguingly, the findings that have emerged to date from large retrospective and prospective clinical studies are not consistent with some of the guiding principles of CTG. For example, the majority of acidemic fetuses do not show suppressed FHRV, and can even show increased FHRV. Moreover, the morphological or timing-based classification of decelerations is not associated with acidemia (cord pH < 7.1), but in contrast the assessment of the depth and duration of all decelerations via metrics such as ‘total deceleration area’ or ‘deceleration capacity’ is associated with acidemia.

These modern clinical findings are not minor tweaks to CTG interpretation, but illustrate that the physiology underlying CTG is not what we were taught to expect. This is paralleled by a much deeper understanding of fetal physiology, through well-designed animal studies. Many of these animal studies involve highly structured sequences of repeated umbilical cord occlusion modelling the intermittent nature of hypoxemia associated with uterine contractions, but are in no way designed to truly reflect the complex and dynamic nature of human labor. Nonetheless, they allow the physiological mechanisms underlying specific features of the FHR trace to be investigated. With these caveats in mind, it is striking that the lessons learned from these animal studies have converged with the lessons from recent clinical studies. For example, animal studies reveal that the regulation of FHRV during labor is complex and cannot be reduced to a binary system in which high equals good and low equals bad, paralleling the inconsistent predictive value of FHRV in clinical studies. Modern understanding of the fetal peripheral chemoreflex (the response to hypoxemia) and the fetal baroreflex also concludes that the peripheral chemoreflex is the most likely mediator of the vast majority of intrapartum decelerations, while the common belief that many decelerations are explained by baroreflex activation is in fact false.
The clinical relevance of this physiological understanding is that the assessment of the depth and duration of all decelerations should provide a broad measure of the total burden of fetal hypoxemia, while the timing of decelerations is a red herring that does not reflect the etiology mediating decelerations in the way it was once thought. Indeed, recent clinical studies have highlighted that metrics consistent with these concepts (total deceleration area and deceleration capacity) are the most predictive metrics identified to date of cord acidemia and outperform traditional timing-based assessment of decelerations4,67.

It is now apparent that we need to be cautious of preconceived ideas about which FHR patterns are associated with fetal wellbeing. A data-driven approach therefore has an important role in the future refinement of CTG and represents the best opportunity to date to retest, reconfirm or refute long-held beliefs about the utility, and even the physiological meaning of FHR patterns.

8. Beyond fetal heart rate: emerging technologies and adoption challenges

Whilst we acknowledge the importance of capturing information on reduction of cerebral blood flow or fetal infection/inflammation, which are recognized precursors of fetal brain injury, we lack the clinical tools to make these observations reliably during labor, directly or indirectly. Preclinical studies however do indicate that inflammatory indices can be developed from heart rate variability derived from the high-precision abdominal ECG that could potentially serve as real-time non-invasive infection biomarker73-75. The clinical adoption challenge to validate these results in prospective studies lies in the currently limited availability and use of the fetal ECG devices (the main motivation to using transabdominal fetal ECG devices remains its superiority for monitoring obese mothers, rather than potential signal-analytical benefits of higher quality fetal ECG signal). The technology is currently available only in few delivery centers with a limited number of devices.

Secondly, there is a resurgence of interest in using fetal EEG monitoring during labor76-78, to make neurological assessment of the fetus. This approach continues initiatives that began more than 40 years ago79,80. Fetal EEG monitoring can be performed using the routine fetal scalp electrode or specially designed electrodes78,81. It represents a clinically testable modality for increasing the accuracy of early detection of fetal acidemia82 or cerebral blood flow79,80. In particular, there appears to be an early response in the fetal EEG to repetitive FHR decelerations accompanied by pathological hypotensive blood pressure responses induced by brief umbilical cord occlusions83 which warrants further investigations.
Finally, to be taken up by practitioners, and to produce a change in health outcomes, the right idea has to arrive at the right time and be met by a technology that can implement it\textsuperscript{52,84,85}. Proving the clinical utility of transabdominal ECG or fetal EEG is a prerequisite to their wider adoption. Although the technologies seem to have arrived, a paradigm shift will likely be required for practitioners to embrace them.

9. **Bringing new monitoring modalities to the market**

Innovations in fetal monitoring and surveillance are difficult to implement into clinical practice for three main reasons. Firstly, maternity departments spend most of their money on personnel rather than investments in technology or medical devices. With budgets for departments decreasing in most of the world, such investment in technology is even more difficult nowadays. Secondly, innovations are hindered by a paradox in the reimbursement system: in countries where hospitals have a revenue per admission or treatment, the net revenue of the maternity department may decrease due to innovations that help reduce the need-to-treat. At the same time, global costs of healthcare would be reduced by successful fetal monitoring innovations, but the cost savings might be made elsewhere in the system – sometimes close to maternity wards, e.g. in neonatology departments; or sometimes much further away, e.g. reduced costs related to care for those with neurological or educational problems. Especially in the latter case, maternity wards are not strongly inclined to invest their already limited budget in innovative technology.

Moreover, to allow reimbursement for new technology, insurance companies and national healthcare systems need to see evidence that cost savings can be made. But without such reimbursement for the new technology, hospitals will often not introduce it in their maternity wards, because of the abovementioned budgeting considerations. This makes it difficult to prove the technology’s cost efficiency or its benefits for the women and newborns. This chicken-and-egg problem can be resolved by clinical trials, but these are subject to multiple drawbacks, some of them specific to the field of fetal monitoring, discussed in detail in Section 5.
Conclusion

The 2\textsuperscript{nd} SPaM Workshop provided a unique and stimulating research forum for academics, clinicians, and industry. We concluded that modern automated algorithms for CTG evaluation perform comparably to each other and to clinical assessment of the CTG (with no clinical context), but the sensitivity and specificity urgently need to be improved. Furthermore, there remains a lack of clarity or consensus about the goal of intrapartum CTG monitoring, in particular, the role of intrapartum acidemia in the etiology of fetal brain injury. From the point of view of developing data-based methodologies, a definition of ‘good’ and ‘bad’ outcomes of labor remains crucial.

We envision that technological progress will arrive in three ways: (1) through better quality and more reliable acquisition of FHR signals; (2) through novel techniques to acquire additional information about the fetus continuously during labor; (3) but mainly through harnessing the power of clinical data at large scale, employing computers to learn and help us understand the relations between FHR, clinical context and neonatal outcomes.

We firmly believe that the computing revolution can meaningfully assist in the development of a long overdue, reliable, continuous means for monitoring fetal health during labor and thus, ultimately, allow the prevention of intrapartum fetal injury where possible. Progress will only be possible with multidisciplinary collaborative research; the availability of large multicenter datasets; funding for research; and carefully designed clinical tests of the new technologies, learning from past mistakes.

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References


15. Georgieva A, Papageorghiou AT, Payne SJ, Moulden M, Redman CWG. Phase-rectified signal averaging for intrapartum electronic fetal heart rate monitoring is related to


72. Westgate JA, Bennet L, Gunn AJ. Fetal heart rate variability changes during brief repeated umbilical cord occlusion in near term fetal sheep. BJOG. 1999;106(7):664-671.


